

FORECAST AND EXPLICATION OF ECG SIGNAL ONGOINGS USING SOFT COMPUTING TECHNIQUES

By

SANTOSH KUMAR SUMAN *

MAYANK KUMAR GAUTAM **

VINOD KUMAR GIRI ***

*-** PG Scholar, Department of Electrical Engineering, Madan Mohan Malaviya University of Technology, Gorakhpur, India.

*** Professor, Department of Electrical Engineering, Madan Mohan Malaviya University of Technology, Gorakhpur, India.

ABSTRACT

The major cause of human loss in Cardiovascular Disease (CVD) is Cardiac problems, that are increasing day-by-day in the world. In order to achieve a great effort and to diagnose the cardiovascular disease, many people use different types of Mobile Electrocardiogram (ECG) in remote monitoring techniques. ECG Feature Extraction acts as an important role in diagnosing most part of the cardiac diseases. Now it has been comprehensively reviewed all way through for feature extraction of ECG signal analyzing, feature extracting, followed by classifying which has been planned a longtime ago. Here the authors have introduced soft computing techniques. To recognize the present situation of the heart, Electrocardiography and is an essential tool, but it is a time consuming process to analyze a continuous ECG signal as it may hold thousands of nonstop heart beats. At this point, the authors convert analog signal in to a digital one, vice versa, and it helps in accurately diagnosing the signal. Aim of this paper is to present a detection of some heat arrhythmias using soft computing techniques.

Keywords: ECG, ANN, BPNN, Arrhythmia, Feature Extraction, Feature Classification.

INTRODUCTION

Electrocardiography deals among the electrical movement of the innermost blood circulatory system, that is the heart. The study of soft computing techniques for ischemia detection in long-duration ECGs are usually divided into three stages. In the first phase, the ECG signal is pre-processed in routing to remove noise. In the second phase, all the important ECG features are extracted and deliberated. Using the above features, in the third phase, each cardiac beat is classified as ordinary or ischemic. Neural Pattern Recognition (NPR) have frequently been used, since the apparatus for realizing the classifiers, which are capable to compacted even with nonlinear bias between the classes and to recognize the unfinished or indistinct input patterns [1-3]. Recently, the connectionist approach has been applied to the ECG analysis with capable results. Electrocardiogram (ECG) represents the electrical movement of the heart. Millions of ECGs were taken for the diagnosis of different classes of patients, and everywhere ECGs can provide a set of issues order about the abnormality in the concerned patient,

which are analyzed by the physicians and interpreted depending ahead their experience. Electrocardiogram (ECG or EKG) is a trace of bio-electric potential dissimilarity recorded throughout the instance on the body surface that represents heart beats [1]. It is clearly described in Figure 1. Every heartbeat cycle is normally characterized

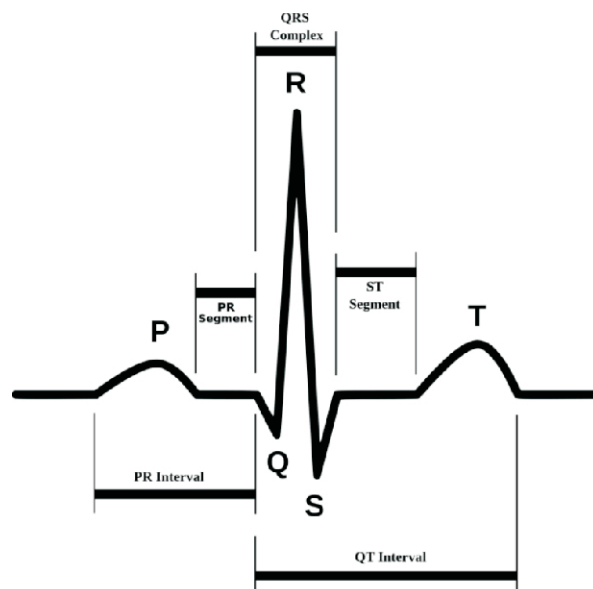


Figure 1. A Sample ECG Signal showing P-QRS-T Wave [5]

by the sequence of waveforms recognized as a P wave, QRS complex and a T wave. Time intervals among people's waveforms as well as their shapes and orientation are demonstrating physiological processes happening in the heart and the autonomous nervous system [4].

Even though nowadays in medical centres, sophisticated equipment and tools are used for detecting the heart-beat arrhythmias and the cardiovascular deformity, visual examination of the multi-channel (lead) ECG record is at rest, which is the first step occupied by cardiologists in the diagnosis procedure. Human heart is separated into four most important chambers called atria and ventricles both with their left and right section. Those chambers jointly structure a biological pump for propelling the blood throughout the body [6-9]. Apart from the four obvious sections, there are some other parts of the heart for very particular functions like dividing atria from ventricles, sluggish impulse circulation, very fast impulse propagation, where all of them perform a particular task, ensuring the proper blood flows efficiently throughout the body. When electrical impulse propagates through the heart and all these specialized cells, ECG electrodes pick up that impulse in various directions and speed. In this way, ECG waveforms are formed [9]. QRS complex is the most noticeable of all the components in electrocardiogram in light of its shape; in this manner, it is taken as a kind of perspective in ECG highlight extraction. Therapeutic finding utilizing Computer frameworks have been produced keeping in mind, the end goal to help medicinal experts in the examination of substantial volumes of patient information which can be separated from the ECG machine. Such procedures work by changing the most subjective analytic criteria into a more target quantitative sign highlight characterization issue [10-15]. The procedures have been utilized to manage this issue, for example, the investigation of ECG signals for the location of electrocardiographic changes, utilizing the autocorrelation capacity, recurrence area highlights, time-recurrence investigation, and the wavelet change. A few techniques comprising of arrangement of band pass channels has a recurrence scope of QRS edifices,

yet these strategies have restricted precision in investigating ECG highlights in the vicinity of high recurrence commotion and additionally the ECG signal influenced by extreme gauge float [15] which should be overcome.

1. Methodology Involved

1.1 Denoising/ Baseline Wander Removal

The noise artifacts rarely that influence the most part of ECG signals is Baseline wandering [16]. Regularly it shows up from breath and lies somewhere around 0.15 and 0.3 Hz. Disposal of Baseline wander is along these lines required in the ECG signal investigation to reduce the inconsistencies in beat morphology. In this paper, the baseline wander of ECG waveform, is dispensed with stacking the first flag first and then smoothen the information in the section vector y utilizing a moving average filter. Results are acquired in the column vector y [17-18]. The authors chosen a range for their work for smoothing the information is 100 for smoothing and it lastly subtracted the smoothed sign from the original signal. Thus, this processed sign is free from baseline drift, which is shown clearly in Figures 2,3,4,5.

1.2 Feature Extraction using Wavelet Transformation

After the elimination of noise, baseline wanders evacuation and peak recognition, it is important to separate the component of the ECG waveform keeping in mind the end goal to utilize it in the next phase of ECG signal investigation [19-21]. The capacity to control and register the information in packed parameters structure is a standout amongst the most vital utilization of wavelet change, are frequently known as components. Highlight extraction is the most vital stride in example acknowledgment. There are a few approaches to remove the elements of an ECG signal. In this work, there are two sort of components extricated for ECG waveforms.

- Morphological component of ECG signal
- Wavelet co-efficient based features

Determination of fitting Feature assumes an imperative part in example acknowledgment. The processed DWT coefficients introduce a conservative representation that

exhibits the vitality conveyance of the sign in time and recurrence [22]. In this stage utilizes daubechies wavelet of request. Hence, the ascertained estimate and the detailed wavelet coefficients of the ECG signs were connected as the element vectors speaking to the signs [23]. Direct utilizing of wavelet coefficient as inputs to the neural system might build the neuron numbers in a concealed layer, which thus harmfully affects the system operation. Keeping in mind, the end goal to minimize the dimensionality of the separated component vectors, the insights of the wavelet coefficients were utilized [24-25]. The accompanying measurable elements were used for the the time-recurrence dispersion of the ECG waveforms:

- Mean of the total estimations of the points of interest and estimate coefficients at every level.
- Standard deviation of the points of interest and estimate coefficients in every level.
- Difference estimations of the points of interest and estimate coefficients at every level.
- Power Spectral Density of ECG Signal.
- The energy of Periodogram of ECG Signal.

At last for each of the ECG signal, 20 wavelet based components have been obtained. Aside from measurable element, the morphological component of an ECG sign is likewise acheived. These elements have most extreme estimations of P, Q, R, S, T tops. Hence the

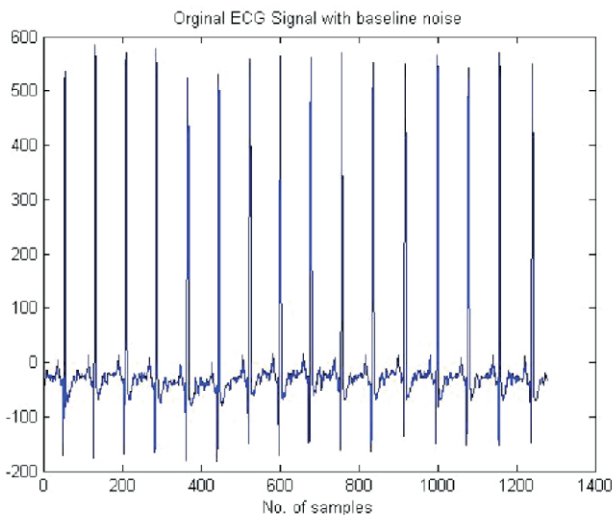


Figure 2. Original ECG Signal with Baseline Noise which has some offset

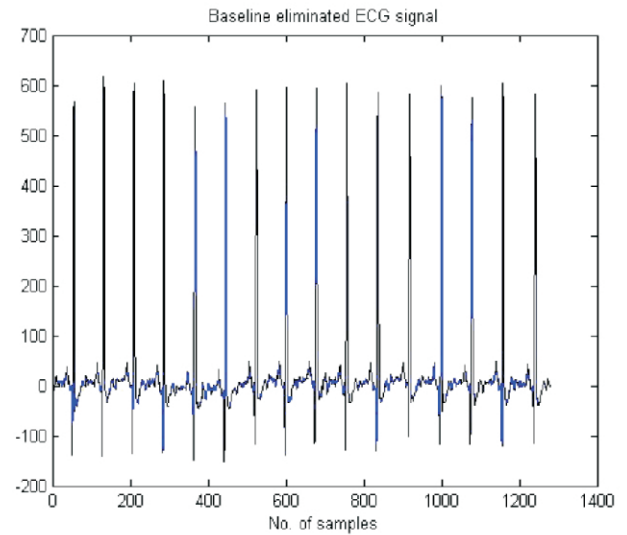


Figure 3. Baseline eliminated ECG Signal which has the offset of 0

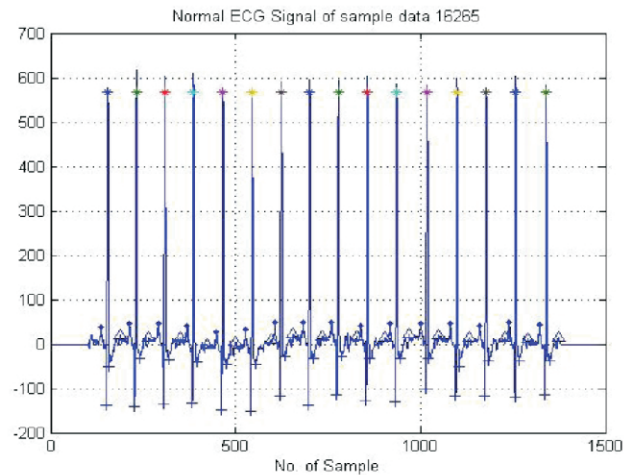


Figure 4. Normal Sample Signal of ECG Data

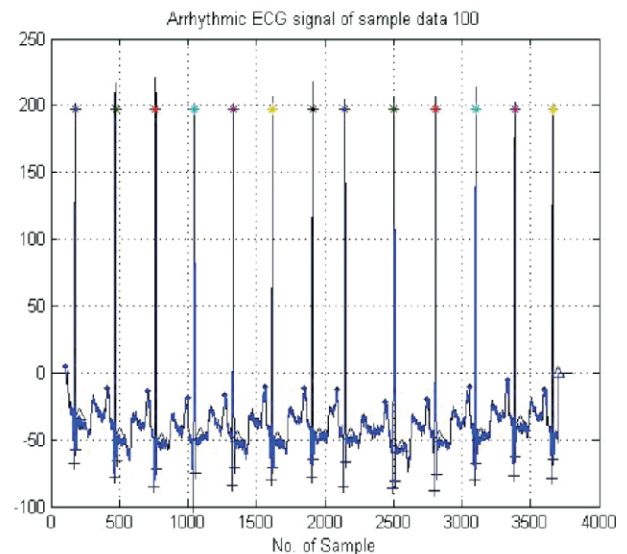


Figure 5. Arrhythmic ECG Signal of Sample Data 100

aggregate have been acquired to apply as a data to the neural system. Following the amounts of the element, a vector might be entirely diverse, and a standardization procedure is required to institutionalize each and every elements to the same level. Normalizing the standard deviation and mean of information allows the system to regard every data as just as fundamental over its scope of qualities [26-28].

1.3 Feature Classification using Neural Networks

Artificial Neural Network (ANN) is a computational model, which is spurred by the structure of biological neural networks. A neural network comprises of an interconnected gatherings of simulated neurons. This paper portrays the utilization of neural network in an example acknowledgment, where the information unit speaks to the component vector and the yield units speaks to the example class, which must be grouped [29-33]. Every info vector (highlight vector) is given to the data layer, and yield of every unit is comparing the component in the vector. Each concealed units ascertains the weighted entirety of its information to blueprint its scalar a net enactment. Net activation is the inward result of the inputs and weight vector at the concealed unit [34].

Results

The MIT-BIH arrhythmia and NSR database is isolated into two separate classes that are normal and arrhythmia. The Each file of ten second recording obtains information and it is isolated into two classes in light of the maximum number of beats sort present on it [35]. Among 67 ECG recordings each of length 30 minutes, just 62 recordings (14 records of ordinary class and 48 from arrhythmia class) of length ten seconds are considered for this work and the record number 19088,19090,19093,19140 and 19830 are not considered in this study. Table 1 demonstrates the

Class	Record Number
Normal Class	16265-16272-16273-16420-16430-16483-16539-16773-16786-16795-17052-17453-18177-18184-19088-19090-19093-19140-19830
Arrhythmia Class	100-101-102-103-104-105-106-107-108-109-111-112-113-114-115-116-117-118-119-121-122-123-124-200-201-202-203-205-207-208-209-210-212-213-214-215-217-219-220-221-222-223-228-230-231-232-233-234

Table 1. Distribution of Records of MIT-BIH NSE & Arrhythmia Database

Type of Sample	No. of Samples	Detection By Neural Network	Accuracy
Normal	14	14	100%
Arrhythmia	48	47	97.91%
Total	62	61	98.38%

Table 2. The Overall Performance of BPNN

used record number from MIT-BIH NSR and arrhythmia database. The aggregate 25 number of components are splitted into two separate classes. These are DWT based elements and morphological component of ECG sign. Following, there are 25 (20 DWT based element and 5 morphological) components that are removed which is given as a data to the BPNN classifier. To recreate and prepare the system, 62 information (14 from typical class and 48 from unusual class) are used. Joining the removed elements, 70% of this information (64 × 25) grid has been accomplished for preparing information and 15% of separated feature (64×25) are utilized for acceptance and staying 15% of extricating highlight lattice data (64×25) are utilized for testing the network.

The simulation result has been obtained by utilizing the Back Propagation Neural Network (BPNN) classifier and the 10 quantities of neurons in the shrouded layer is utilized for preparing and testing the ECG signal. Two neurons are utilized at the yield layer of the system as (1, 0) and (0, 1) alluding to normal and arrhythmia class. Table 2 shows the overall performance of BPNN.

Conclusion

In this paper, the authors had discussed about different methods and algorithms for highlighting the feature extraction of ECG signal. Likewise, it ought to be exceedingly precise and ensure quick extraction of elements from the ECG signal and then just it is productive. Closer the premise capacity catches the sign attributes, the more smaller is the representation, furthermore, more probable are the components touchy to the important ECG states and heartless to varieties in unessential clamor. In this part, the authors have redone the fundamental elements of a consistent wavelet representation by picking polynomial wavelet premise works that match the qualities of a fiducially 1-beat long ECG signal example separated from the Poincare

segmenting of ECG signal pattern. The customized representations were observed to be around two requests of extent more minimized (measured in term of sign entropy) than the wavelet premise capacities accessible in the standard wavelet library. In spite of the fact that, we can effectively characterize the heart arrhythmias. This work uncovers that, the abnormality location of the ECG signal taking into account discrete wavelet change and BPNN is 100% effective. They have arranged the MIT-BIH NSE and arrhythmia database records into ordinary and arrhythmia classes in view of the sorts of ECG beats present in it. Out of 68 records, the 62 records of ten second recording are considered for characterizing the ECG signal, while the remaining 5 records are rejected for this study. Since, aggregate 62 records and 25 elements are utilized as a part of this study to order the sign. The authors have accomplished general exactness of 98.4% utilizing back engendering neural system (BPNN) with 10 quantities of neurons in the concealed layer. The outcome for preparing and testing the ordinary and arrhythmia information test is more prominent than 90% utilizing BPNN classifier, which demonstrates the enhanced proficiency of the proposed work.

References

- [1]. Hari Mohan Rai, and Anurag Trivedi, (2012). "Classification of ECG Waveforms for Abnormalities Detection using DWT and Back Propagation Algorithm". *International Journal of Advanced Research in Computer Engineering & Technology*, Vol. 1, No. 4.
- [2]. S. Osowski, and T.H. Linh, (2001). "ECG beat recognition using fuzzy hybrid neural network". *IEEE Trans. Biomed. Eng.* Vol. 48, pp. 1265-1271.
- [3]. Maedeh Kiani Sarkaleh and Asadollah Shahbahrami, (2012). "Classification of ECG arrhythmias using discrete wavelet transform and neural networks". *IJCSEA*, Vol. 2, No. 1.
- [4]. K. Minami, H. Nakajima and T. Toyoshima, (1999). "Real-Time discrimination of ventricular tachyarrhythmia with fourier-transform neural network". *IEEE Trans. on Biomed. Eng.* Vol. 46, pp.179-185.
- [5]. I. Romero and L. Serrano, (2001). "ECG frequency domain features extraction: A new characteristic for arrhythmias classification". in *Proc. 23rd Annual Int. Conf. on Engineering in Medicine and Biology Society*, pp. 2006-2008.
- [6]. P. de Chazal, M. O'Dwyer and R. B. Reilly, (2000). "A comparison of the ECG classification performance of different feature sets". *IEEE Trans. on Biomed. Eng.* Vol. 27, pp. 327-330.
- [7]. P. de Chazal, M. O'Dwyer and R. B. Reilly, (2004). "Automatic classification of heartbeats using ECG morphology and heartbeat interval features". *IEEE Trans. on Biomed. Eng.* Vol. 51, pp. 1196-1206.
- [8]. C. Alexakis, H. O. Nyongesa, R. Saatchi, N. D. Harris, C. Davis, C. Emery, R. H. Ireland and S. R. Heller, (2003). "Feature extraction and classification of electrocardiogram (ECG) signals related to hypoglycemia". *Proc. Computers in Cardiology*, Vol. 30, pp. 537-540.
- [9]. P. Ivanov, M. QDY, R. Bartsch, et al, (2009). "Levels of complexity in scaleinvariant neural signals". *Physical Review*.
- [10]. N. Srinivasan, D.F. Ge, S.M. Krishnan, "Autoregressive Modeling and Classification of Cardiac Arrhythmias". *Proceedings of the Second Joint Conference*, TX, USA.
- [11]. Hafizah Hussain, Lai Len Fatt, (2007). "Efficient ECG Signal Classification Using Sparsely Connected Radial Basis Function Neural Network". *Proceeding of the 6th WSEAS International Conference on Circuits, Systems, Electronics, Control and Signal Processing*, pp. 412-416.
- [12]. Marcel R. Risk, Jamil F. Sobh, and J. Philip Saul, (1997). "Beat Detection and Classification of ECG using Self Organizing Maps". *Proceedings of 19th International Conference - IEEEEMBS*, Chicago, IL, USA
- [13]. Yuksel Ozbay, Rahime Ceylan, and Bekir Karlik, (2011). "Integration of type-2 fuzzy clustering and wavelet transform in a neural network based ECG classifier". *Expert Systems with Applications*, Vol. 38, pp. 1004-1010.
- [14]. Physionet. *The MIT-BIH Arrhythmia Database*: Retrieved from <http://physionet.ph.biu.ac.il/physiobank/database/mitdb/>
- [15]. R. Mark and G. Moody, *MIT-BIH Arrhythmia Database*

Directory. Retrieved from <http://ecg.mit.edu/dbinfo.html>

[16]. Hari Mohan Rai, and Anurag Trivedi, (2012). "De-noising of ECG waveforms using multiresolution wavelet transform". *International Journal of Computer Application*, Vol. 45, No.18.

[17]. Michel Misiti, Yves Misiti, Georges Oppenheim, and Jean-Michel Poggi, (1996). "Wavelet Toolbox for use with MATLAB". Vol. 1.

[18]. A. R. Sahab, and Y. Mehrzad Gilmalek, (2011). "An Automatic Diagnostic Machine for ECG Arrhythmias classification Based on Wavelet Transformation and Neural Networks". *International Journal of Circuits, Systems and Signal Processing*, Vol. 5, No. 3.

[19]. Richard O. Duda, Peter E Hart David G Stork, (2002). *Pattern Classification: II Edition*, John Wiley.

[20]. Mathworks. *Neural Network Toolbox*. Retrieved from <http://www.mathworks.com>

[21]. L. Khadra, A. Fraiwan, and W. Shahab, (2002). "Neural-wavelet analysis of cardiac arrhythmias". *Proceedings of the WSEAS International Conference on Neural Network and Applications (NNA '02)*, Interlaken, Switzerland, pp.3241-3244.

[22]. Qian Zheng, Chao Chen, and Zhinan Li, (2013). "A Novel Multi-Resolution SVM (MR-SVM) Algorithm to detect ECG signals anomaly". in *WE-CARE Project – Center for Wireless Communication and Signal Processing*.

[23]. Sarikal, P. and Wahidabanu, R., (2010). "Robust R peak & QRS detection in electrocardiogram using wavelet transform". (*IJACSA*) *International Journal of Advanced Computer Science Applications*, Vol.1(6), pp. 48-53.

[24]. Gothwal, H., Kedawat, S., & Kumar, R. (2011). "Cardiac arrhythmias detection in an ECG beat signal using fast Fourier transform and artificial neural network". *Journal of Biomedical Science & Engineering*, Vol. 4(4), pp. 289-296.

[25]. Qibin Zhao and Liqing Zhan, (2005). "ECG Feature Extraction and Classification Using Wavelet Transform and Support Vector Machines". *International Conference on Neural Networks and Brain, ICNN & B*, Vol. 2, pp. 1089-

1092.

[26]. Awadhesh Pachauri, and Manabendra Bhuyan, (2009). "Robust Detection of R-Wave Using Wavelet Technique". *World Academy of Science, Engineering and Technology*, Vol. 56.

[27]. Ashley EA, and Niebauer J., (2004). *Conquering the ECG*. London: Remedica.

[28]. F.A Davis, (2005). *ECG notes*.

[29]. V. S. Chouhan, and S. S. Mehta, (2008). "Detection of QRS Complexes in 12- lead ECG using Adaptive Quantized Threshold". *IJCSNS International Journal of Computer Science and Network Security*, Vol. 8, No. 1.

[30]. M.B. Tayel, and Mohamed E. El-Bouridy, (2006). "ECG Images Classification Using Feature Extraction Based On Wavelet Transformation and Neural Network". *ICGST, International Conference on AIML*.

[31]. P. Tadejko, and W. Rakowski, (2007). "Mathematical Morphology Based ECG Feature Extraction for the Purpose of Heartbeat Classification". *6th International Conference on Computer Information Systems and Industrial Management Applications, CISIM'07*, pp. 322-327.

[32]. F. Sufi, S. Mahmoud, and I. Khalil, (2008). "A new ECG obfuscation method: A joint feature extraction & corruption approach". *International Conference on Information Technology and Applications in Biomedicine*, pp. 334-337.

[33]. S.C. Saxena, A. Sharma, and S.C. Chaudhary, (1997). "Data compression and feature extraction of ECG signals". *International Journal of Systems Science*, Vol. 28, No. 5, pp. 483-498.

[34]. Emran M. Tamil, Nor Hafeezah Kamarudin, Rosli Salleh, M. Yamani Idna Idris, Noorzaily M. Noor, and Azmi Mohd Tamil, (2008). "Heartbeat Electrocardiogram (ECG) Signal Feature Extraction Using Discrete Wavelet Transforms (DWT)".

[35]. E.D. Übeyli, (2009). "Detecting variabilities of ECG Signals by Lyapunov Exponents". *Neural Computing and Applications*, Vol.18, No. 7, pp. 653-662.

[36]. Alan Jovic, and Nikola Bogunovic, (2007). "Feature Extraction for ECG Time- Series Mining based on Chaos

Theory". Proceedings of 29th International Conference on Information Technology Interfaces.

ABOUT THE AUTHORS

Santosh Kumar Suman graduated from the Azad Institute of Engg & Technology Lucknow (Uttar Pradesh Technical University, Lucknow), India with B.Tech degree in Electrical Engineering in 2013 and currently pursuing his M.Tech in Control & Instrumentation at MMMUT, Gorakhpur, India. His research interests include Intelligent Techniques, Optimization Technique, and Control System.



Mayank Kumar Gautam obtained his B.Tech. (Electrical & Electronics Engg.) Hons. (Medalist) Degree from R.R. Institute of Modern Technology, Lucknow (Affiliated to Gautam Buddh Technical University) Lucknow (UP) in 2012. Presently, he is pursuing M.Tech (Control & Instrumentation) in the Department of Electrical Engineering at Madan Mohan Malaviya University of Technology (erstwhile Madan Mohan Malaviya Engineering College), Gorakhpur (UP). Published three research papers in International Referred Journals and three research papers in IEEE Conferences. His research interests include Digital Signal Processing (Medical Signal Processing), Measurement and Instrumentation, Biomedical Instrumentation and Engineering, ECG and Control Systems.



V.K. Giri obtained his B.E. (Electrical) Degree from REC, Surat (Gujrat) in 1988, M.E. (Measurement and Instrumentation) Hons. degree from University of Roorkee, Roorkee in 1997 and Ph.D. degree from Indian Institute of Technology Roorkee, in 2003. He joined the Department of Electrical Engineering at M.M.M Engineering College, Gorakhpur (UP) in 1989 as a lecturer. Presently, he holds the position of Professor in the same department since, 2008. He has published more than 50 research papers, guided 14 PG students; and supervising 6 Ph.D. theses. He has received many awards including the Best Paper awards of the Institution of Engineers (India) in 23rd Indian Engineering Congress in the year 2008. He was elected as a Fellow of the Institution of Engineers (I), Institution of Electronics and Telecommunication. Engineers, and is a member of many professional bodies such as Life Member of ISTE, Member IEE and Member CSI. He has also undertaken large number of consultancy, testing & sponsored projects from industries and government departments. His research interests include Digital Signal Processing, Measurement and Instrumentation, Biomedical Instrumentation, ECG, Data Compression and Telemedicine.

